Title: Gray matter hypertrophy and thickening with obstructive sleep apnea in middle-aged and older adults

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Author’s contributions: Ms. Baril contributed to the study’s conception and design and to data acquisition, analysis, and interpretation; she drafted the paper and revised it following the author’s comments. Ms. Gagnon and Ms. Brayet contributed to the study’s design, to data acquisition and interpretation, and to critical revision of the work. Drs. De Beaumont, Montplaisir, Lafond, Carrier, and Gagnon contributed to the study’s conception and to data interpretation, and revised the work critically. Mr. L’Heureux contributed to data acquisition and analysis, and revised the work critically. Dr. Gosselin contributed to the study’s conception and design and to data interpretation; she also helped draft the paper and revised it critically. All authors approved the final version for publication and are accountable for all aspects of the work.

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At a Glance Commentary:
*Scientific Knowledge on the Subject:* Older individuals with obstructive sleep apnea are at risk of presenting cognitive decline and dementia. While previous studies investigated cerebral gray matter structure in obstructive sleep apnea, inconsistencies exist regarding the presence of changes and their specific locations in the brain. Furthermore, there is a lack of understanding regarding gray matter integrity in the aging population with obstructive sleep apnea since very few studies specifically evaluated this age group.

*What This Study Adds to the Field:* This study assessed the relationship between intrinsic markers of obstructive sleep apnea severity and multiple measures of cerebral gray matter structure in a large sample of middle-aged and older individuals. We found that the main markers of obstructive sleep apnea severity are related to increased thickness and/or volume of the frontal, parietal, and cingulate regions of the cortex as well as the amygdala. These results suggest that obstructive sleep apnea in the aging and mostly presymptomatic population is associated with underlying cerebral adaptive/reactive mechanisms.

This article has an online data supplement, which is accessible from this issue's table of content online at [www.atsjournals.org](http://www.atsjournals.org)
Abstract

**Rationale:** Obstructive sleep apnea causes intermittent hypoxemia, hemodynamic fluctuations, and sleep fragmentation, all of which could damage cerebral gray matter that can be indirectly assessed with neuroimaging.

**Objectives:** To investigate whether markers of obstructive sleep apnea severity are associated with gray matter changes among middle-aged and older individuals.

**Methods:** Seventy-one subjects (ages: 55 to 76; apnea–hypopnea index: 0.2 to 96.6 events/h) were evaluated with magnetic resonance imaging. Two techniques were used: 1) voxel-based morphometry, which measures gray matter volume and concentration; 2) FreeSurfer automated segmentation, which estimates the volume of predefined cortical/subcortical regions and cortical thickness. Regression analyses were performed between gray matter characteristics and markers of obstructive sleep apnea severity (hypoxemia, respiratory disturbances, sleep fragmentation).

**Measurements and Main Results:** Subjects had few symptoms, i.e. sleepiness, depression, anxiety and cognitive deficits. While no association was found with voxel-based morphometry, FreeSurfer revealed increased gray matter with obstructive sleep apnea. Higher levels of hypoxemia correlated with increased volume and thickness of the left lateral prefrontal cortex as well as increased thickness of the right frontal pole, the right lateral parietal lobules, and the left posterior cingulate cortex. Respiratory disturbances positively correlated with right amygdala volume while more severe sleep fragmentation was associated with increased thickness of the inferior frontal gyrus.

**Conclusions:** Gray matter hypertrophy and thickening were associated with hypoxemia, respiratory disturbances, and sleep fragmentation. These structural changes in a group of middle-
aged and older individuals may represent adaptive/reactive brain mechanisms attributed to a presymptomatic stage of obstructive sleep apnea.

**Keywords:** Sleep-Disordered Breathing, Aging, Neuroimaging, Hypoxemia, Cerebral Cortex.

**Number of words in the abstract:** 249 words
Main text

Introduction

Repetitive airway collapses in obstructive sleep apnea (OSA) lead to chronic cycles of hypoxemia/reoxygenation and hypercapnia, hemodynamic fluctuations, and sleep fragmentation (1). According to animal models, these pathophysiological processes have consequences on the brain by provoking oxidative stress, cellular death and cellular morphological modifications (2-4). Consequently, OSA may lead to structural cerebral gray matter changes. Considering that OSA is particularly common in the aging population (1) and is a risk factor for accelerated cognitive decline (5) and dementia (6), the relation between gray matter integrity and OSA severity in the older population must be assessed to deepen our understanding of its contribution to neurodegeneration.

In OSA, gray matter volume has been investigated predominantly in middle-aged adults using voxel-based morphometry (VBM). A recent meta-analysis showed that OSA correlates with a smaller parahippocampal and fronto-temporal cortex (7). However, due to variations between studies (e.g. VBM pipeline, apnea-hypopnea index [AHI] thresholds), others argue that there is currently no clear evidence of gray matter atrophy (8).

Since the sole use of VBM resulted in inconsistencies, its combination with alternative morphometric techniques could lead to a clearer picture of gray matter integrity in OSA. Few studies used other analysis techniques and gray matter characteristics. Regional cortical thinning and reduced gray matter concentration were reported in middle-aged individuals with OSA (9, 10). Moreover, segmentation of predefined subcortical structures in OSA individuals showed gray matter atrophy (hippocampi, mammillary bodies, caudate nuclei) (11-13) but also
hypertrophy (hippocampi, putamen) (14, 15).

It is unclear whether OSA leads to altered structural gray matter integrity. This is especially true in the older population with OSA for whom gray matter integrity has not been assessed thoroughly. The present study focuses on late middle-aged and older individuals, and investigates the association between OSA severity and gray matter characteristics estimated with different analysis techniques: volume and concentration measured with VBM; and cortical thickness and cortical/subcortical volume assessed with FreeSurfer automated segmentation. Instead of groups based on an arbitrary criterion to define OSA, we used a regression approach on a large sample with varying levels of OSA severity. The novelty of the study resides in the fact that it combines multiple analysis techniques and gray matter characteristics in association with multiple markers of OSA severity (hypoxemia, respiratory disturbances, and sleep fragmentation).

We hypothesized that all markers of OSA severity, but more particularly hypoxemia, would be linked to reduced gray matter in regions known to be sensitive to pathological processes observed in OSA (e.g. hippocampus and surrounding structures, prefrontal cortex) (1). We also hypothesized that an alternative method to VBM, namely FreeSurfer automated segmentation, could be more sensitive to reveal how OSA affects specific brain regions. Preliminary results have been previously reported in abstract form (16).

**Methods**

An online supplement describes the protocol in detail. The study included 71 subjects who were either healthy controls or newly diagnosed and untreated individuals with OSA. Thirty-seven of them (52%) participated in a previous study on cerebral perfusion in OSA (17). Ten subjects were recruited from a clinic for suspected OSA while the remaining subjects were
recruited through newspapers advertisements. Exclusion criteria were neurological, pulmonary, and major psychiatric diseases; sleep disorders other than OSA; OSA treatment including continuous positive airway pressure; uncontrolled diabetes and hypertension; morbid obesity; and medication affecting cerebral functioning. The Ethics Committees (#2012-697 and #12-13-008) approved the research protocol and written consent was obtained from each subject.

Subjects were evaluated with an all-night in-laboratory polysomnographic recording and 3-Tesla magnetic resonance imaging (MRI). Although the AHI is generally thought to represent OSA severity, its sole use has been challenged (18). Indeed, other variables related to oxygen saturation and sleep quality are also recognized as correlates of OSA severity. A principal component analysis was therefore used to extract independent markers of OSA severity, to reduce the number of statistical tests, and to prevent the multi-collinearity problem of highly correlated variables in a regression. Respiratory and sleep variables that strongly correlate with the AHI ($p < 0.001$) were included in the principal component analysis. Although less-correlated variables could be of interest, they may not fully reflect OSA pathophysiology and are not as well suited for a principal component analysis. Resulting rotated and uncorrelated components represented hypoxemia, respiratory disturbances, and sleep fragmentation (see Table 1).

Figure 1 depicts the neuroimaging analysis techniques used, i.e., VBM and FreeSurfer automated segmentation. VBM was performed in accordance with published recommendations (8). T1-weighted MRI images were processed with the VBM8 toolbox (http://www.neuro.uni-jena.de/) within SPM8 (http://www.fil.ion.ucl.ac.uk/spm/software/spm8/). Default processing options were used to run the pipeline, including a spatial normalization that deformed every subject into a common space. The pipeline was run once with and once without modulation, which rescales images and transforms gray matter concentration into volume (19). A multiple regression design within SPM8 was performed between markers of OSA severity (hypoxemia,
respiratory disturbances, and sleep fragmentation) and both gray matter volume and concentration, adjusted for age, sex, body mass index, and intracranial volume. Level of significance was set at \( p < 0.05 \), clusters corrected for multiple comparisons with topological false-discovery rate.

MRI images were also processed using FreeSurfer (http://surfer.nmr.mgh.harvard.edu/), which features the volumetric segmentation of subcortical structures (20) and the parcellation of the cortical surface (21) without a deforming spatial normalization. Cortical/subcortical volume and cortical thickness values from predefined brain regions were extracted for each subject. Hierarchical linear regressions for extracted FreeSurfer values were performed with age, sex, body mass index, and intracranial volume as covariates (Step 1) and with markers of OSA severity (hypoxemia, respiratory disturbances, and sleep fragmentation; Step 2). Level of significance was set at \( p < 0.01 \) for \( R^2 \) changes, i.e., the increase in variance explained by adding OSA variables to covariates, and \( p < 0.01 \) for predicting markers of OSA severity.

**Results**

1. *Clinical characteristics of the sample*

Seventy-eight subjects were evaluated with an MRI. A neuroradiologist inspected the MRI images, which led to the exclusion of six subjects for major abnormalities such as silent infarcts or large arachnoid cysts. Another subject was excluded due to a processing problem, for a total of seven exclusions after the MRI.

The final sample was composed of 71 subjects ranging in age from 55 to 76 (mean age: 65.3 ± 5.6 years). Although the objective of the study was answered with a regression design
across the complete sample, subjects were divided into four groups based on their AHI and one-way ANOVAs were performed to better characterize our sample’s characteristics (see Table 2). Healthy control subjects (AHI <5) represented 17% of the sample, 42% were included in the mild OSA group (AHI between ≥5 and <15), 16% were included in the moderate OSA group (AHI between ≥15 and <30), and 25% were individuals considered to have severe OSA (AHI ≥30). The AHI varied from 0.2 to 96.6 events/h and 35% of the final sample had an OSA-related complaint and/or had suspected OSA before joining the study (e.g., snoring, daytime sleepiness, lack of energy, bed partner witnessing respiratory disturbances).

Groups were statistically comparable for the Epworth Sleepiness Scale, the Beck Depression and Anxiety Inventories, the Montreal Cognitive Assessment, the Mini-Mental State Examination, and the Index of Vascular Burden (see Table 2). Markers of OSA severity extracted with the principal component analysis (see Table 1) did not correlate with any of these questionnaires and tests. In fact, a minority of mild to severe OSA subjects had excessive daytime sleepiness (33% with Epworth Sleepiness ≥10), depressive symptoms (26% with Beck Depression Inventory II ≥10), anxiety symptoms (12% with Beck Anxiety Inventory ≥10) and cognitive deficits (16% with Montreal Cognitive Assessment <26). In summary, this suggests that our participants were not highly symptomatic in terms of sleepiness, mood, and global cognition, and that this symptomatology was not related to OSA severity. Moreover, a minority of OSA subjects was obese (25% with a body mass index ≥30 kg/m²) or had more than one cardiovascular risk factor and disease (31% with an Index of Vascular Burden >1).

2. **Gray matter hypertrophy and thickening with OSA severity**

VBM revealed no significant association between OSA severity and clusters of gray matter volume or concentration at a false-discovery rate corrected threshold ($p <0.05$).

Conversely, with FreeSurfer automated segmentation, significant regression models
revealed increases, but no decrease, in cortical thickness and volume associated with markers of OSA severity (see Table 3, Figure 2, and Figure E1 of the online supplement). The majority of significant models were of increased cortical thickness in relation to the level of hypoxemia. More severe hypoxemia was associated with increased thickness of the left rostral middle frontal gyrus, the right frontal pole, the right superior and inferior parietal lobules, and the left posterior cingulate cortex. Hypoxemia levels were also positively correlated with the volume of the left pars orbitalis portion of the inferior frontal gyrus. Moreover, higher levels of respiratory disturbances were associated with a hypertrophic right amygdala whereas an increased level of sleep fragmentation was correlated with a thicker pars triangularis region of the right inferior frontal gyrus.

3. **Complementary results of gray matter hypertrophy and thickening with OSA severity**

Interestingly, similar positive associations were observed at a trend level with FreeSurfer (R² change between p <0.05 and p >0.01; predicting OSA components p <0.01; β values between 0.24 and 0.40) for contralateral cortical regions in relation to hypoxemia levels (thickness of the right rostral middle frontal gyrus, left inferior parietal lobule, and right posterior cingulate cortex) as well as for subcortical regions in association with more respiratory disturbances (volume of the left amygdala, hippocampus, and thalamus).

To assess whether gray matter structure is associated with markers of OSA severity even in milder forms of OSA, analyses were conducted among control subjects and mild to moderate groups (AHI <30). With FreeSurfer, increased gray matter was found in relation to hypoxemia in several fronto-parietal regions and respiratory disturbances in left thalamus and precuneus (see online supplement).
**Discussion**

This study investigated the association between markers of OSA severity and gray matter integrity in untreated individuals aged 55 and over. We found that higher levels of hypoxemia during sleep were associated with increased volume and/or thickness of the prefrontal, parietal, and cingulate regions of the cortex. Moreover, a higher number of respiratory disturbances was associated with an enlarged amygdala whereas a more fragmented sleep was correlated to a thicker frontal cortex. Our hypothesis was only partially confirmed since we predicted that atrophied gray matter would be associated with increased OSA severity. The novelty of this study lies not only in its results, but also in the use of specific markers of OSA severity in relation with multiple cerebral gray matter characteristics.

1. **Potential mechanisms underlying gray matter increases with OSA severity**

It would be surprising that gray matter increases underlie better neuron viability or neurogenesis. Indeed, neurogenesis in the adult brain is less probable outside the hippocampus, the subventricular zone and the olfactory bulb (22). Gray matter hypertrophy and thickening may instead result from cerebral edema, a well-known effect of hypoxemia that can be observed after only 16 h in protocols imitating altitude in humans (23). Consistently, a diffusion MRI study in individuals with newly diagnosed OSA suggested the presence of vasogenic edema in subcortical structures (24). In addition to edema, hypoxia causes changes in cellular size or quantity with the potential to enlarged gray matter. In fact, studies on rodents subjected to intermittent hypoxia during their sleep (1 to 10 days and 5 weeks respectively) showed increased brain water content, branching of surviving neurons, as well as astroglial hyperplasia and/or hypertrophy (i.e., reactive gliosis) (3, 25). Increased gray matter in relation to hypoxemia levels could also be representative
of early neurodegeneration processes. Multiple animal models of hypoxic exposure (from few hours to several days) consistently showed increased β-amyloid generation (1), a pathogenic mechanism of Alzheimer’s disease. β-amyloid deposition in the absence of abnormal tau levels was recently reported to correlate with increased cortical thickness (26).

Overall, intermittent hypoxemia is probably a key mechanism leading to cerebral edema, cellular responses and early neurodegeneration in gray matter. This is consistent with our findings since most regions with increased gray matter were associated with hypoxemia levels. Similarly, hypoxemia strongly correlated with gray matter increases even when subjects with severe OSA were removed from the analysis, confirming that milder forms of OSA are also associated with gray matter changes in our sample. At the clinical level, it suggests that intermittent hypoxemia may be particularly important to consider when making decision for treatment, even in patients with AHI below 30.

In addition to the relationship between hypoxemia and gray matter characteristics, respiratory disturbances and sleep fragmentation were also associated with gray matter hypertrophy or thickening in the present study. Changes in breathing pattern due to obstructions and sleep fragmentation were shown to be both independently associated with blood pressure fluctuations (27, 28), which could lead to cerebral edema (29). Furthermore, experimental obstructive apneas and sleep fragmentation may distinctly provoke cellular responses through various mechanisms, such as cerebral oxidative stress (2, 4). However, the specific effects of respiratory disturbances and sleep fragmentation are less understood than the effects of intermittent hypoxemia.

2. **Increases versus decreases of gray matter structure in OSA**

Although the existing literature mostly reports gray matter losses among individuals with
OSA (7-13), gray matter hypertrophy has also been observed (14, 15, 30-32). The same pattern is shown with the effect of OSA treatment on gray matter. In one set of studies, treatment led to gray matter hypertrophy, suggesting a recovery from atrophic processes (33, 34), while others showed that OSA treatment reduced either regional gray matter or whole brain volume (31, 35), suggesting reversal of hypertrophic processes such as brain edema.

Increased gray matter may represent a presymptomatic stage of the OSA disease process where its severity is characterized by reactive and adaptive brain mechanisms, such as cerebral edema, reactive gliosis, neuronal branching, and increased β-amyloid deposition. Later in the disease progression, gray matter atrophy could represent predominantly neuronal damage due to chronic OSA and lead to cognitive decline. Both adaptive and maladaptive effects on the brain have consistently been described for processes that follow cycles of airway obstructions and reoxygenation (36). Our sample had low levels of symptoms, namely sleepiness, mood and cognitive deficits, which reflect that most subjects were in a presymptomatic stage of OSA that may be characterized by more adaptive brain responses and thus, increased gray matter. Obviously, these hypotheses must be confirmed.

OSA duration might affect the balance between adaptive and maladaptive mechanisms, but it is generally unknown. In hypoxic rodent and human protocols that observed mechanisms that could underlie increased gray matter, exposure to hypoxia was relatively short (from a few hours to several days) (1, 3, 23, 25). Gray matter hypertrophy and thickening could therefore be present in an earlier stage of the disease, although duration of hypoxic exposure in rodent and human protocols is difficult to translate to OSA in a clinical setting.

Age could also determine whether atrophy or hypertrophy is observed in reaction to OSA. In fact, OSA in older adults is possibly different in terms of mechanisms, comorbidities, consequences, and symptoms compared to younger patients. Age is associated with partially
protective mechanisms against OSA, such as reduced production of oxidative stress following apneas (37) and decreased blood pressure and heart rate responses following arousals (38). Adaptive effects of hypoxia on the brain could lead to relative cerebrovascular protection and reduced mortality risk in subjects over age 50 with OSA compared to their younger counterparts (39). Therefore, a different response to OSA could occur with age and its severity may be correlated with increases in gray matter structure. Very few studies have specifically evaluated gray matter in subjects over age 50. These had very different designs and objectives, and thus, diverging results (40-42). Therefore, how OSA impacts the aging brain must be clarified.

3. **Vulnerability of specific brain regions to OSA**

In the present study, markers of OSA severity were associated with increased thickness or volume in the lateral prefrontal cortex, the parietal lobules, and posterior cingulate cortex as well as the amygdala. Interestingly, previous studies on OSA showed both increased and decreased gray matter volume and/or thickness in the same or adjacent regions as those reported in the present study (9, 11, 13-15, 30-32, 43, 44). Therefore, these regions may be especially vulnerable to OSA and be preferentially affected by both swelling and atrophic processes. It is also important to highlight that we found trends for association between OSA markers of severity and increased gray matter in contralateral brain regions. It would be interesting to follow this cohort in order to verify whether these trends will reach significance over time.

Hypoxemia and sleep fragmentation correlated with the structure of the lateral prefrontal cortex in our study. It has been suggested that the prefrontal cortex is vulnerable to both hypoxemia and sleep disruption in OSA (45). In addition, our results showed that hypoxemia was associated with core constituents of the default mode network, namely the parietal and posterior cingulate regions of the cortex. The metabolic activity of these highly connected regions
fluctuates together (46) and their elevated oxygen demand could make them more vulnerable to hypoxemia (47). Finally, we found that amygdala volume was linked to respiratory disturbances, which is consistent with its altered activity during a respiratory challenge in OSA subjects (48).

4. Utility of complementary gray matter analysis techniques and characteristics

While the most widely used technique for gray matter analysis is VBM, we observed no changes with this method, a result supported by previous studies on OSA (35, 49). VBM has limitations including misregistration and reduced accuracy of region location (19). This might be exacerbated by ventricular expansion caused by global atrophy in normal aging, in which processing errors could lead to false results in regions surrounding the ventricles. FreeSurfer automated segmentation may be more sensitive in detecting early changes in OSA than a voxel-based approach, since volume and thickness are computed by region without a prior spatial normalization. Instead, the brain is labeled and segmented in an automated manner similar to manual volumetry (20, 21), which probably represent more closely the real structure. However, FreeSurfer automated segmentation is time-consuming and depends on predefined atlases.

VBM and FreeSurfer segmentation show results on different scales. While VBM investigates the brain voxel by voxel (1.5 mm³), the predefined regions extracted with FreeSurfer are much larger. This suggests that increases in gray matter with OSA severity are subtle and diffuse across a given brain structure, which could have been missed in some previous VBM studies. In addition, more regions of increased thickness than volume were observed with FreeSurfer, a result that may also have been missed with VBM. Overall, FreeSurfer automated segmentation and its measurement of cortical thickness seems to be more sensitive to detect gray matter increases with OSA severity than VBM. However, our results must be replicated by further studies in the older population with OSA.
5. **Strengths and limitations**

Our large sample size of 71 subjects with an AHI varying from 0.2 to 96.6 events/h represent the entire spectrum of OSA severity, which allowed a regression approach. This eliminated the need for an arbitrary criterion to define the presence of the condition that is necessary for a between-group design, leading to inconsistencies between studies. A regression design also allowed us to investigate different markers of OSA severity. Moreover, the use of different analysis techniques and gray matter characteristics yielded a more complete evaluation of gray matter in OSA.

Nonetheless, the fact that most of our subjects were not severely hypoxic (see Table 2) and were mostly presymptomatic restricts the generalization of our results to other individuals with OSA. Although our strict exclusion criteria facilitate the interpretation of our findings by excluding many confounding conditions, they could limit the generalization of our results to individuals presenting OSA and comorbidities.

Although we included sex as a nuisance covariate, women with OSA may present more maladaptive than adaptive cerebral processes. In fact, compared to males with comparable OSA severity, females have impaired white matter integrity (50). Since we investigated only 16 females (23% of our sample), this could explain the difference between our results and the study by Celle et al. (40), which showed brainstem atrophy among mostly women (64%) in a similar age group.

6. **Conclusions**

Our study revealed that markers of OSA severity, i.e. hypoxemia, respiratory disturbances, and sleep fragmentation, are linked to increases in cortical thickness and gray matter volume that are more sensitively detected with a technique alternative to VBM, namely FreeSurfer automated segmentation. OSA severity, especially hypoxemia, could contribute to gray matter hypertrophy
and thickening through local edema and reactive cellular responses. These structural changes in frontal, parietal, and cingulate regions of the cortex and in the amygdala may be possible in presymptomatic and/or older subjects with OSA, among whom more adaptive than maladaptive mechanisms may occur. Longitudinal investigations are needed to determine whether increased gray matter structure will later show atrophy and be associated with cognitive decline in order to deepen our understanding of the link between OSA and neurodegeneration in the aging population.
Acknowledgements

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Figure Legends

Figure 1. Processing steps for estimating gray matter characteristics using VBM (A) and FreeSurfer (B). T1-weighted MRI images were used for both VBM and FreeSurfer analyses. In order to conduct VBM analyses (A), images were first segmented and normalized into a common space. A non-linear modulation was performed to obtain volume and final volume and concentration images were smoothed. In summary, the VBM processing pipeline segments and deforms gray matter to allow inter-subject comparisons for both gray matter concentration and volume in every voxel. For FreeSurfer analyses (B), non-brain tissues were first removed and a
registration was performed. The brain was segmented according to voxel intensities and a probabilistic atlas to extract subcortical volumes. White- and gray matter boundaries were traced and the cortex was parcelled and labeled based on folding pattern and a probabilistic atlas. Thus, FreeSurfer outputs are undeformed cortical/subcortical volume as well as cortical thickness of regions predefined by built-in atlases. Overall, both analysis techniques work differently to estimate gray matter characteristics: with VBM, the brain was deformed and gray matter was compare at each voxel. With FreeSurfer automated segmentation, gray matter values are averaged over regions labeled in the undeformed brain according to built-in atlases. VBM images and FreeSurfer extracted values correspond to final processed variables used in multiple regression analyses with markers of OSA severity. FWHM, full-width half maximum; MRI, magnetic resonance imaging; VBM, voxel-based morphometry; OSA, obstructive sleep apnea.

Figure 2. Locations of increased gray matter estimated with FreeSurfer automated segmentation in association with markers of OSA severity. Hypoxemia [1] was positively correlated with the volume of the left pars orbitalis of the inferior frontal gyrus and the thickness of the left rostral middle frontal gyrus, the left posterior cingulate cortex, and the right frontal pole, as well as the right superior and inferior parietal lobules. Moreover, higher levels of
respiratory disturbances [2] were associated with a larger right amygdala while more severe sleep fragmentation [3] was correlated with an increased thickness of the right pars triangularis of the inferior frontal gyrus. Regression analyses included age, sex, body mass index, and intracranial volume as nuisance covariates. OSA, obstructive sleep apnea.
Footnotes

Footnotes for Table 1.

Bold variables show how variable loads on each rotated component. Loadings >0.5 were considered to be variables that contribute the most to the component. OSA, obstructive sleep apnea; SpO₂, oxygen saturation; TST, total sleep time; NREM1, non-rapid eye movement sleep stage 1.

Footnotes for Table 2.

Results are presented as mean (standard deviation). OSA, obstructive sleep apnea; AHI, apnea–hypopnea index; F, females; TST, total sleep time; SpO₂, oxygen saturation; NREM1, non-rapid eye movement sleep stage 1. * X² tests were performed between groups; † p <0.05; ‡ p <0.001.

Footnotes for Table 3.

Bold variables show the predicting OSA component for each region of increased gray matter. OSA, obstructive sleep apnea; BMI, body mass index; ICV, intracranial volume; ΔR²; R² change; R, right; L, left. *p <0.01; †p <0.005.
### Table 1. Markers of OSA severity obtained with a principal component analysis of respiratory and sleep variables.

<table>
<thead>
<tr>
<th>Respiratory and sleep variables</th>
<th>Hypoxemia</th>
<th>Respiratory disturbances</th>
<th>Sleep fragmentation</th>
</tr>
</thead>
<tbody>
<tr>
<td>Minimal SpO₂ (%)</td>
<td>-0.867</td>
<td>-0.330</td>
<td>-0.188</td>
</tr>
<tr>
<td>TST with SpO₂ &lt;90% (min)</td>
<td>0.815</td>
<td>0.408</td>
<td>0.175</td>
</tr>
<tr>
<td>Apnea–Hypopnea Index (events/h)</td>
<td>0.389</td>
<td>0.877</td>
<td>0.221</td>
</tr>
<tr>
<td>TST in apnea–hypopnea (%)</td>
<td>0.401</td>
<td>0.852</td>
<td>0.265</td>
</tr>
<tr>
<td>Micro-arousal index (events/h)</td>
<td>-0.002</td>
<td>0.404</td>
<td>0.816</td>
</tr>
<tr>
<td>Number of stage transitions to NREM1 and wakefulness</td>
<td>0.437</td>
<td>0.050</td>
<td>0.803</td>
</tr>
<tr>
<td>Accounted variance (%)</td>
<td>32.0%</td>
<td>32.3%</td>
<td>24.9%</td>
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</table>
Table 2. Clinical and polysomnographic characteristics of healthy control, mild, moderate and severe OSA groups.

<table>
<thead>
<tr>
<th>Variables</th>
<th>Groups</th>
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<th>Post-hoc tests</th>
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<tr>
<td></td>
<td>Control</td>
<td>Mild</td>
<td>Moderate</td>
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<td></td>
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<tr>
<td>Number of subjects</td>
<td>n = 12</td>
<td>n = 30</td>
<td>n = 11</td>
</tr>
<tr>
<td>Sex* (#F; %F)</td>
<td>2F; 16.7%</td>
<td>10F; 33.3%</td>
<td>1F; 9.1%</td>
</tr>
<tr>
<td>Age (years)</td>
<td>62.3 (4.7)</td>
<td>65.8 (5.9)</td>
<td>65.9 (5.1)</td>
</tr>
<tr>
<td>Body mass index (kg/m²)</td>
<td>26.5 (3.9)</td>
<td>26.5 (3.1)</td>
<td>27.9 (2.1)</td>
</tr>
<tr>
<td>Epworth Sleepiness Scale</td>
<td>6.5 (4.8)</td>
<td>7.2 (4.8)</td>
<td>9.7 (4.8)</td>
</tr>
<tr>
<td>Beck Depression Inventory</td>
<td>3.2 (3.7)</td>
<td>5.3 (4.9)</td>
<td>6.2 (5.2)</td>
</tr>
<tr>
<td>Beck Anxiety Inventory</td>
<td>4.3 (5.3)</td>
<td>3.1 (3.3)</td>
<td>3.2 (4.5)</td>
</tr>
<tr>
<td>Montreal Cognitive Assessment</td>
<td>27.4 (2.4)</td>
<td>27.5 (2.0)</td>
<td>27.5 (2.4)</td>
</tr>
<tr>
<td>Mini-Mental State Examination</td>
<td>28.1 (2.3)</td>
<td>29.0 (1.0)</td>
<td>28.2 (1.8)</td>
</tr>
<tr>
<td>Index of Vascular Burden</td>
<td>0.8 (0.8)</td>
<td>1.0 (1.1)</td>
<td>1.0 (0.9)</td>
</tr>
<tr>
<td>% hypercholesterolemia*</td>
<td>25.0</td>
<td>36.7</td>
<td>36.4</td>
</tr>
<tr>
<td>% hypertension*</td>
<td>41.7</td>
<td>40.0</td>
<td>54.6</td>
</tr>
</tbody>
</table>

Respiratory variables

| AHI (events/h) | 2.1 (1.5) | 9.2 (2.5) | 22.2 (4.8) | 45.1 (19.5) | 180.8‡ | A < B < C < D |
| TST in apnea–hypopnea (%) | 1.2 (1.1) | 5.7 (2.0) | 12.8 (1.9) | 31.5 (15.5) | 147.8‡ | A < B < C < D |
| Mean SpO₂ (%) | 95.5 (0.6) | 94.6 (1.2) | 93.7 (0.7) | 94.2 (1.2) | 6.1† | A > C, D |
| Minimal SpO₂ (%) | 90.5 (3.3) | 88.5 (3.3) | 83.6 (3.8) | 81.5 (5.9) | 16.3‡ | A, B > C, D |
| TST with SpO₂ < 90% (min) | 0.1 (0.1) | 2.0 (5.7) | 5.5 (3.8) | 17.6 (18.6) | 26.2‡ | A, B < C, D |

Sleep variables

<p>| TST (min) | 369.2 (60.7) | 341.5 (64.5) | 370.9 (43.9) | 368.5 (46.0) | 1.4 |
| Wake duration (min) | 100.8 (44.6) | 101.3 (57.5) | 80.2 (46.4) | 91.6 (54.0) | 0.6 |</p>
<table>
<thead>
<tr>
<th></th>
<th>78.5 (9.0)</th>
<th>77.2 (12.6)</th>
<th>82.6 (9.1)</th>
<th>80.6 (10.0)</th>
<th>0.8</th>
</tr>
</thead>
<tbody>
<tr>
<td>Sleep efficiency (%)</td>
<td>12.0 (3.9)</td>
<td>14.3 (6.1)</td>
<td>14.3 (5.7)</td>
<td>25.2 (11.2)</td>
<td>8.8‡</td>
</tr>
<tr>
<td>Micro-arousal index (events/h)</td>
<td>56.9 (19.2)</td>
<td>55.1 (15.0)</td>
<td>66.8 (19.0)</td>
<td>97.8 (41.8)</td>
<td>9.6‡</td>
</tr>
<tr>
<td># of stage transitions to NREM1 and wakefulness</td>
<td>A, B, C &lt; D</td>
<td>A, B &lt; D</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>
Table 3. Significant hierarchical linear regressions between markers of OSA severity and regions of increased gray matter volume and thickness segmented automatically with FreeSurfer.

<table>
<thead>
<tr>
<th>Brain regions</th>
<th>Step 1: Nuisance covariates</th>
<th>Step 2: OSA severity</th>
<th>Respiratory disturbances</th>
<th>Sleep fragmentation</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Age</td>
<td>Sex</td>
<td>BMI</td>
<td>ICV</td>
</tr>
<tr>
<td><strong>Subcortical volume</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>R amygdala</td>
<td>R² 31.9%†</td>
<td>47.9%†</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>16.0%†</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>β</td>
<td>-0.07</td>
<td>0.01</td>
<td>0.05</td>
</tr>
<tr>
<td><strong>Cortical volume</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>L pars orbitalis (inferior frontal)</td>
<td>R² 11.8%</td>
<td>30.0%†</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>18.3%†</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>β</td>
<td>-0.03</td>
<td>0.05</td>
<td>-0.08</td>
</tr>
<tr>
<td><strong>Cortical thickness</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>L rostral middle frontal gyrus</td>
<td>R² 8.9%</td>
<td>29.4%†</td>
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</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>20.5%†</td>
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</tr>
<tr>
<td></td>
<td>β</td>
<td>-0.24</td>
<td>-0.02</td>
<td>0.11</td>
</tr>
<tr>
<td>R frontal pole</td>
<td>R² 0.0%</td>
<td>19.1%</td>
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<td></td>
</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>18.8%†</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>β</td>
<td>0.00</td>
<td>-0.00</td>
<td>0.03</td>
</tr>
<tr>
<td>R pars triangularis (inferior frontal)</td>
<td>R² 6.5%</td>
<td>22.9%</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>16.5%*</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>β</td>
<td>-0.16</td>
<td>0.11</td>
<td>0.18</td>
</tr>
<tr>
<td>R superior parietal lobule</td>
<td>R² 7.7%</td>
<td>24.3%</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>ΔR²</td>
<td>16.7%*</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>β</td>
<td>-0.11</td>
<td>0.03</td>
<td>0.22</td>
</tr>
<tr>
<td>R inferior</td>
<td>R² 3.8%</td>
<td>20.8%</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Region</td>
<td>$\Delta R^2$</td>
<td>$R^2$</td>
<td>$\Delta R^2$</td>
<td>$\beta$</td>
</tr>
<tr>
<td>----------------------</td>
<td>---------------</td>
<td>--------</td>
<td>---------------</td>
<td>----------</td>
</tr>
<tr>
<td>Parietal lobule</td>
<td>17.0%*</td>
<td></td>
<td></td>
<td>-0.17</td>
</tr>
<tr>
<td>L posterior cingulate cortex</td>
<td>5.9%</td>
<td>23.7%</td>
<td>17.8%†</td>
<td>-0.08</td>
</tr>
</tbody>
</table>